

In Vitro Comparison of Aerosol Characteristics of HFA Ipratropium Bromide Pressurized Metered Dose Inhaler (pMDI) Formulation from Three Valved Holding Chambers (VHCs)

K. Nikander¹, L. Slator², D. von Hollen¹, R.H.M. Hatley². ¹Philips Respironics, Respironics New Jersey, Inc., Parsippany, New Jersey, USA. ²Respironics Respiratory Drug Delivery (UK) Ltd, Chichester, UK.

Introduction



Figure 1. The OptiChamber Diamond VHC can be used to optimize delivery from pMDIs.

The valved holding chamber (VHC) has been designed to help improve and optimize delivery for those using pressurized metered dose inhalers (pMDIs).^[1] The OptiChamber Diamond VHC (Diamond; Philips Respironics, Respironics New Jersey, Inc., Parsippany, NJ) is a compact, anti-static^[2] VHC designed to facilitate effective aerosol delivery to respiratory patients. The *in vitro* aerosol characteristics of an HFA ipratropium bromide pMDI with a preproduction Diamond VHC were compared with those of the pMDI with an AeroChamber Plus Z-Stat (Z-Stat, Monaghan Medical Corp., Plattsburgh, NY) VHC, an AeroChamber Plus (AC+, Monaghan Medical Corp.) VHC and the pMDI alone.

Method

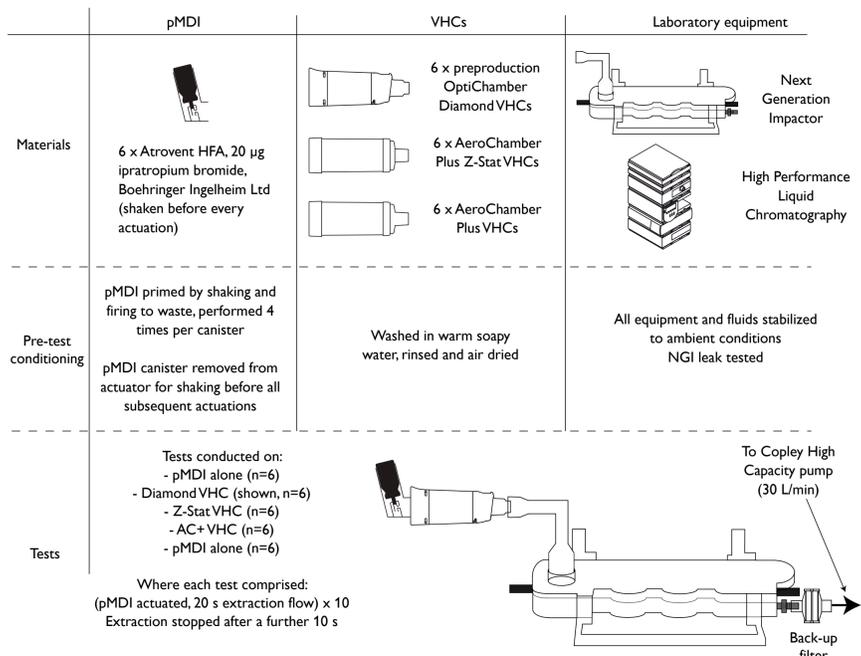


Figure 2. Experimental test method.

After each test the induction port, back-up filter, NGI cups and VHCs were processed using HPLC assay diluent. CITDAS V3.10 software was used to generate the aerosol characteristics data. The mean emitted dose (drug entering NGI), fine particle dose (amount of drug in NGI $\leq 4.7 \mu\text{m}$), fine particle fraction (percentage of emitted dose in particles $\leq 4.7 \mu\text{m}$), and Mass Median Aerodynamic Diameter (MMAD) were calculated. The equipment was washed and dried after each drug/VHC test.

Results

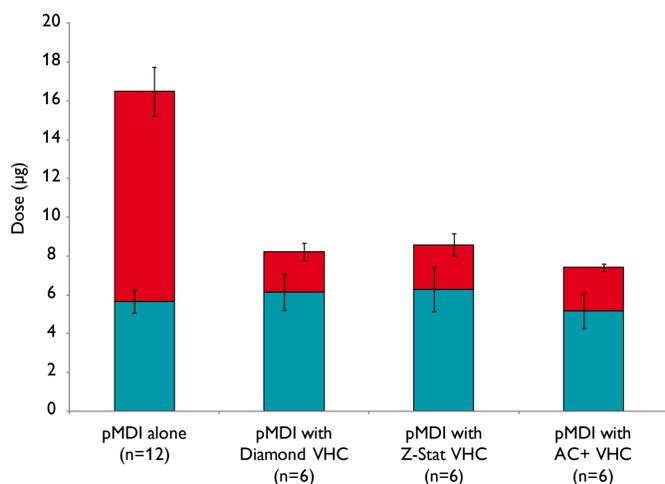


Figure 3. Emitted dose (drug entering the NGI) from the pMDI alone, pMDI with Diamond VHC, pMDI with Z-Stat VHC and pMDI with AC+ VHC with the fine particle dose highlighted ■ and the dose in particles $> 4.7 \mu\text{m}$ highlighted ■. Error bars denote standard deviation about the mean.

The dose emitted from each device comprised of the fine particle dose (particles $\leq 4.7 \mu\text{m}$) and the dose in particles $> 4.7 \mu\text{m}$ in diameter. Although the emitted dose for the pMDI alone was greater than for the pMDI VHC combinations, Figure 3 shows that this difference was derived from a difference in particles $> 4.7 \mu\text{m}$ in diameter. In fact the large particle dose was over twice as large as the fine particle dose for the pMDI alone. This implies that the VHCs retained a large proportion of particles over $4.7 \mu\text{m}$ in size, which would otherwise have been deposited in the throat and upper stages of the impactor.

The dose emitted from the AC+ VHC was slightly lower than the dose emitted from the anti-static VHCs.

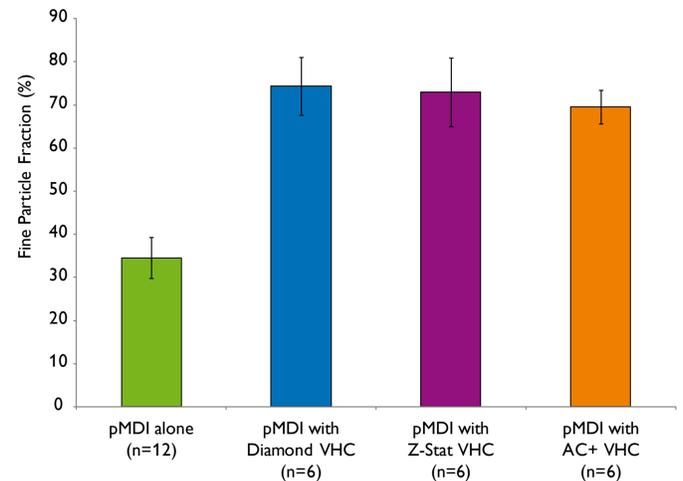


Figure 4. Fine particle fraction (percentage of the emitted dose in particles $\leq 4.7 \mu\text{m}$) from the pMDI alone, pMDI with Diamond VHC, pMDI with Z-Stat VHC and pMDI with AC+ VHC. Error bars denote standard deviation about the mean.

When the results are expressed in terms of fine particle fraction (the percentage of the emitted dose in particles $\leq 4.7 \mu\text{m}$) as in Figure 4, aerosol delivery from the pMDI alone is shown to be less efficient than from the pMDI VHC combinations for the delivery of drug to the lungs. That is, the proportion of the total aerosolized drug that would be expected to penetrate the upper airways and deposit in the conducting and alveolated airways is higher for the pMDI VHC combinations compared with the pMDI alone.^[3]

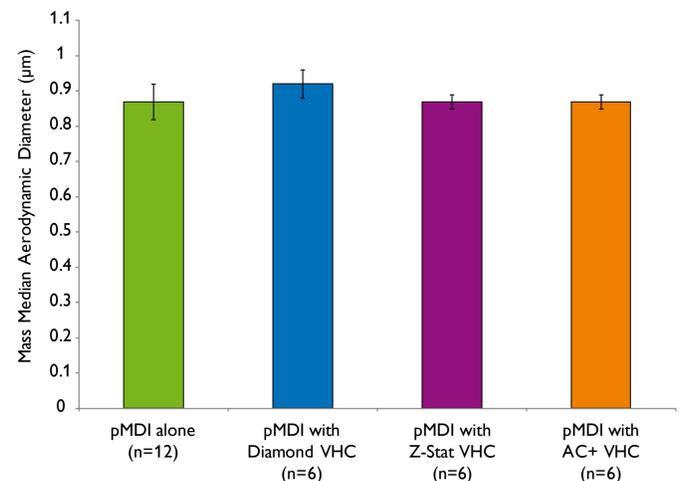


Figure 5. Mass Median Aerodynamic Diameter of the aerosol from the pMDI alone, pMDI with Diamond VHC, pMDI with Z-Stat VHC and pMDI with AC+ VHC. Error bars denote standard deviation about the mean.

The MMAD of aerosol from the pMDI alone and each pMDI VHC combination was similar.

Discussion

The fine particle dose from the pMDI alone and pMDI VHC combinations was similar, but the emitted dose was higher for the pMDI alone, meaning a greater amount of drug was delivered in larger particles that would be expected to deposit in the throat and upper airways.^[3] The aerosol delivery characteristics from the three pMDI VHC combinations were comparable.

Conclusions

- The aerosol delivery characteristics were similar from the VHCs when washed before use and used to deliver HFA ipratropium bromide.
- The fine particle fraction was higher using a pMDI VHC combination than the pMDI alone due to the VHC potentially retaining large particles, which could reduce the oropharyngeal deposition in patients using a pMDI.

References

- Virchow J.C., Crompton G.K., Dal Negro R., Pederson S., Magnan A., Seidenberg J., Barnes P.J. Importance of inhaler devices in the management of airway disease. *Respir Med.* 2008;102:10-19.
- Pierart F., Wildhaber J.H., Vrancken I., Devadason S.G., Le Souëf P.N. Washing plastic spacers in household detergent reduces electrostatic charge and greatly improves delivery. *Eur Respir J.* 1999;13:673-678.
- Heyder J., Gebhart J., Rudolf G., Schiller C.F., Stahlhofen W. Deposition of particles in the human respiratory tract in the size range of 0.0005 – 15 µm. *J Aerosol Sci.* 1986; 17(5):811-815.

Acknowledgements: Editorial assistance was provided by L. Pearce and N. Smith of P55 Consultants Ltd.

Presented at the European Respiratory Society Conference, 24th-28th September 2011, Amsterdam, The Netherlands.

